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Multiphase modeling of porous media from concrete to tumor growth

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Concrete at early age

- Outline of the general mathematical model
- Relevant hydration-dependent constitutive relationships
- Applications: massive structures and repairs

Tumor growth

General conclusions

Massive structures

TCM models



Other concrete structures

.

Thin structures





HCM models

Assumptions **unidirectional coupling THC**→**M**:

- partial saturation
- small displacements and small crack opening

Peculiarities of the model

- Effect of age on the desorption isotherm and Biot's coefficient
- Autogenous and drying shrinkage computed in a unified way
- Mechanical damage coupled with creep
- 3D implementation in Cast3M that simplifies model exploitation

Background:

Gawin D., Pesavento F., Schrefler B. (2006) Benboudjema F. and Torrenti J-M (2008)



The MULTIPHASE system

Concrete is treated as a **porous solid** and porosity is denoted by ε , so that the volume fraction occupied by the solid skeleton is $\varepsilon^{s}=1-\varepsilon$.

The rest of the volume is occupied by the liquid water (ε ^{*I*}); and the gaseous phase (ε ^{*g*}).



1 Solid phase s:	 Anhydrous cement: <i>Cs</i> Aggregates: <i>As</i> Hydrates: <i>Hs</i> 		
1 Liquid phase <i>l</i> :	• Liquid water		
1 Gaseous phase g:	 Water vapour: Wg Dry air: Ag 		

Mass exchanges $\stackrel{\alpha \to \beta}{M}$ and reaction terms $\mathcal{E}^{s} r^{Hs}$



 $\mathcal{E}^{s}r^{Hs}$ hydration rate of the anhydrous cement

 $\stackrel{l \to H_s}{M}$ chemically combined water and $\stackrel{l \to W_g}{M}$ vaporized water *per* second

Mass balance equations: SOLID PHASE [s]



Mass balance equations: LIQUID PHASE [/]

$$\frac{\partial \left(\varepsilon^{l} \rho^{l}\right)}{\partial t} + \nabla \cdot \left(\varepsilon^{l} \rho^{l} \mathbf{v}^{\bar{l}}\right) = -\overset{l \to Hs}{M} - \overset{l \to Wg}{M}$$

Mass balance equations: GAZEOUS PHASE [g]

Vapour water:

$$\frac{\partial \left(\varepsilon^{g} \rho^{g} \omega^{W_{g}}\right)}{\partial t} + \nabla \cdot \left(\varepsilon^{g} \rho^{g} \omega^{\overline{W_{g}}} \mathbf{v}^{\overline{g}}\right) + \nabla \cdot \left(\varepsilon^{g} \rho^{g} \omega^{\overline{W_{g}}} \mathbf{u}^{\overline{W_{g}}}\right) = \overset{l \to W_{g}}{M}$$

Dry air:

$$\frac{\partial \left(\varepsilon^{g} \rho^{g} \omega^{\overline{Ag}}\right)}{\partial t} + \nabla \cdot \left(\varepsilon^{g} \rho^{g} \omega^{\overline{Ag}} \mathbf{v}^{\overline{g}}\right) + \nabla \cdot \left(\varepsilon^{g} \rho^{g} \omega^{\overline{Ag}} \mathbf{u}^{\overline{Ag}}\right) = 0$$

Summing the previous two equations gives:

$$\frac{\partial \left(\varepsilon^{g} \rho^{g}\right)}{\partial t} + \nabla \cdot \left(\varepsilon^{g} \rho^{g} \mathbf{v}^{\bar{g}}\right) = \overset{l \to Wg}{M}$$

Governing equations

Primary variables: $p^g p^c T \mathbf{u}$ Internal variables: ΓD



ENTHALPY BALANCE EQUATION:

$$\left(\rho C_{p}\right)_{\text{eff}} \frac{\partial T}{\partial t} - \nabla \cdot \left(\boldsymbol{\chi}_{\text{eff}} \nabla T\right) = L_{hydr} \frac{\mathrm{d}\Gamma}{\mathrm{d}t} + H_{vap} \frac{\partial \left(\varepsilon^{l} \rho^{l}\right)}{\partial t} + H_{vap} \frac{M}{M} - H_{vap} \nabla \cdot \left[\rho^{l} \frac{k_{rel}^{l} \mathbf{k}}{\mu^{l}} \nabla \left(p^{g} - p^{c}\right)\right]$$

LINEAR MOMENTUM BALANCE EQUATION:

$$\nabla \cdot \left(\frac{\partial \mathbf{t}}{\partial t}\right) + \frac{\partial \rho}{\partial t} \mathbf{g} = 0$$

The hydration model

$$\Gamma_{(t)} = \frac{m_{(t)}^{hydr}}{m_{\infty}^{hydr}}$$

Degree of reaction (hydration advancement)

With: $m_{(t)}^{hydr}$ chemically combined water mass at time t

 m_{∞}^{hydr} chemically combined water mass at time $t = \infty$

Arrhenius type law with the rate of hydration is a function of:

- Hydration degree
- relative humidity
- temperature

$$\frac{d\Gamma}{dt} = A_{(\Gamma)}\beta_{(h)}\exp\left(-\frac{E_a}{RT}\right)$$

 $\begin{array}{ll} A_{(\Gamma)} & chemical affinity \\ \beta_{(h)} & function of relative humidity [0 - 1] \\ E_a & activation energy \end{array}$

Volume fractions of phases during hydration

T.C. Power model (Enhanced by Jensen and Hansen to account silica fume, 2001)

Chemical shrinkage:	$V_{cs} = k \cdot \left[0, 20 + 0, 69 \cdot \left(s/c\right)\right] \cdot \left(1 - p\right) \cdot \xi$	Coment paste
Capillary water:	$V_{cw} = p - k \cdot \left[1, 32 + 1, 57 \cdot (s/c)\right] \cdot (1-p) \cdot \xi$	
Gel water:	$V_{gw} = k \cdot \left[0, 60 + 1, 57 \cdot (s/c)\right] \cdot (1-p) \cdot \xi$	
Gel solid:	$V_{gs} = k \cdot \left[1,52+0,74\cdot(s/c)\right] \cdot (1-p) \cdot \xi$	 Porosity function Solf designation
Cement:	$V_c = k \cdot (1-p) \cdot (1-\xi)$	 Autogenous shrinkage
Silica fume:	$V_{cs} = k \cdot \left[1, 43 \cdot (s/c)\right] \cdot (1-p) \cdot (1-\xi)$	obtained from stochiometry
$k = \frac{1}{1 + (\rho_c/\rho_s) \cdot (s/c)}$	$p = \frac{w/c}{(w/c) + (\rho_w/\rho_c) + (\rho_w/\rho_s) \cdot (s/c)}$	

w, *c* and *s* are respectively the masses of water, cement and silica fume present in a cubic meter of concrete.



Hydration degree and LeChatelier contraction

25%

Hydration-dependent desorption isotherm



Visco-elastic damageable model



Shrinkage computed consistently with the effective stress principle of porous media mechanics.

$$\xrightarrow{\alpha p^{s}} \xrightarrow{E} \xrightarrow{k_{bc1}} \eta_{bc2} \eta_{dc} \xrightarrow{\alpha p^{s}} \prod_{\eta_{bc1}} \eta_{bc1}$$

$$\dot{\tilde{\mathbf{t}}} = \mathbf{E}_{(\Gamma)} \dot{\mathbf{e}}_{el} = \mathbf{E}_{(\Gamma)} \left(\dot{\mathbf{e}} - \dot{\mathbf{e}}_{th} - \dot{\mathbf{e}}_{cr} - \dot{\mathbf{e}}_{sh} \right)$$



$$\mathbf{t}_{eff} = \mathbf{\tilde{t}} + \mathbf{1}\alpha p^{s}$$

Biot's coefficient

$$\alpha = 1 - K_T / K_S$$

Mechanical properties vs hydration degree



*This law is used for **Young's modulus**, **tensile strength** and **fracture energy.**

The damage model

Tensile branch of the t-e relationship (J. Mazars)



The damage model

Four points bending test



ConCrack Benchmark*



CEOS.fi





RG8: Large specimen with restrained shrinkage

DESCRIPTION OF THE TEST

The longitudinal strains of the structure are globally restrained by two struts.

-During the first 2 days after the cast, the structure is isolated.

-Then the isolation and the formwork are removed and the structure is conserved during 2 months in the environment

-Therefore after this two months, the structure is submitted to a static bending test.

**ConCrack* (2011) is an international benchmark for Control of Cracking in reinforced concrete structures. This benchmark is part of the national French project <u>CEOS</u> (*Comportement et Evaluation des Ouvrages Speciaux vis-à-vis de la fissuration et du retrait*) dedicated to the analysis of the behaviour of special construction works concerning cracking and shrinkage.

ConCrack Benchmark



From the left to the right: image of the structure, finite element mesh of the concrete and of the reinforcement bars (a). Adiabatic calorimetry test (b). Evolution of the Young's modulus with time (c). Autogenous (d) and total (e) shrinkage tests. Loss of mass test (f). Loss of mass versus drying shrinkage (g).

ConCrack Benchmark: THC results





- (a) Specimen orientation;
- (b) Temperature 2,25 days after the cast (afternoon);
- (c) Experimental and numerical results for the temperature in the central point of the beam.

ConCrack Benchmark: MEC results





Modeling of a repaired beam



Three identical reinforced beams* are considered. Two of these beams, after the hydrodemolition of 30 mm of the upper part, had been repaired: one using the **ordinary concrete (OC)** and the other using the **ultra-high performance fiber reinforced concrete (UHPC)**. The third beam is the reference specimen.

*These repaired beams are real cases analyzed experimentally by Bastien Masse (2010).

Modeling of a repaired beam





Modeling of a repaired beam RELATIVE HUMIDITY AND SATURATION DEGREE





Vertical displacement of the middle points of the three beams (point D).



3-points bending test

(C)

-Ref.

20

- · Rep. OC

--- Rep. UHPC

25

30



(a) Beam repaired using the UHPC. Only some racks are traversing





Experimental crack pattern

(b) Force versus averaged strain of the compressed fiber optic sensor.

(c) Force versus displacement curves (numerical results).





General conclusions

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STAGES OF TUMOR GROWTH



The MULTI-PHASE system

FOR AVASCULAR TUMOR GROWTH

4 PHASES ARE CONSIDERED

The system consists of the extra-cellular matrix, **ECM**, modeled as a solid phase, and three immiscible fluid phases: the tumor cell population **TC**, the host cell population **HC**, and the interstitial fluid **IF**.



The MULTI-PHASE system

FOR AVASCULAR TUMOR GROWTH

We model IF, HC and TC as fluids: 3-phase flow with interfacial properties Diffuse interface model: interfaces are present throughout the domain



Cell migration in a 3D extracellular matrix Gabriel G. Martins and John Kolega (2006) Surface tension of cell aggregates varies between 1x10⁻³ and 22x10⁻³ N/m

Ambrosi et al. 2012

Surface tension of water 72x10⁻³ N/m

Volume fractions

Volume fractions occupied by the different phases:



Model derivation and its solution

- Mass balance equations of phases and species;
- Linear momentum balance equations of phases;
- Constitutive relationships to close the model;
- Numerical solution and computational strategy.

Mass exchanges $M^{\alpha \to \beta}$ and reaction terms $\mathcal{E}^{s} r^{Hs}$





$$LTC: \frac{\partial \left[\varepsilon'\rho'\left(1-\omega^{Ni}\right)\right]}{\partial t} + \nabla \cdot \left[\varepsilon'\rho'\left(1-\omega^{Ni}\right)\mathbf{v}^{i}\right] + \varepsilon'r^{Nt} - \overset{i \to t}{M} = 0$$

$$NTC: \frac{\partial \left(\varepsilon'\rho'\omega^{Ni}\right)}{\partial t} + \nabla \cdot \left(\varepsilon'\rho'\omega^{Ni}\mathbf{v}^{i}\right) - \varepsilon'r^{Nt} = 0$$
Summing these two eqs gives
$$TS\left[t\right]: \frac{\partial \left(\rho'\varepsilon S^{t}\right)}{\partial t} + \nabla \cdot \left[\rho'\varepsilon S^{t}\mathbf{v}^{t}\right] - \overset{l \to t}{\underset{growth}{S}} = 0$$

$$IF\left[t\right]: \frac{\partial \left(\rho'\varepsilon S^{t}\right)}{\partial t} + \nabla \cdot \left(\rho'\varepsilon S^{t}\mathbf{v}^{t}\right) + \overset{l \to t}{\underset{growth}{M}} = 0$$
Summing over all species gives
$$Mass balance of species in IF$$

$$\frac{\partial \left(\varepsilon'\rho'\omega^{\overline{i}}\right)}{\partial t} + \nabla \cdot \left(\varepsilon'\rho'\omega^{\overline{i}}\mathbf{v}^{\overline{i}}\right) + \nabla \cdot \left(\varepsilon'\rho'\omega^{\overline{i}}\mathbf{u}^{\overline{i}}\right) + \overset{l \to t}{M} = 0$$

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$$\mathbf{TCs}[t]: \frac{\partial \left(\rho^{t} \varepsilon S^{t}\right)}{\partial t} + \nabla \cdot \left[\rho^{t} \varepsilon S^{t} \mathbf{v}^{t}\right] - M_{growth}^{t \to t} = 0$$

$$\mathbf{G}_{1} \cdot \mathbf{G}_{2}$$

$$\begin{array}{c} 0,80-1,00\\ 0,60\\ 0,80\\ 0,60\\ 0,40\\ 0,20\\ 0,00\end{array} \xrightarrow{Pressure in the TCs phase} 0,00-0,20 \\ 0,00 \xrightarrow{Pressure in the TCs phase} 0,00 \xrightarrow{Pressure in the TCs$$

Pressure saturation relationships

Interfaces are capable to sustain a pressure difference

Each of the three fluids of the multiphase system has its specific pressure, p^{α} , so a pressure difference exists between any pair of fluid phases:



$$p^{hl}(S^{t}) = a \tan\left[\frac{\pi}{2}(1-S^{t})^{b}\right]$$
$$p^{th}(S^{t}) = a\frac{\sigma_{th}}{\sigma_{hl}} \tan\left[\frac{\pi}{2}(S^{t})^{b}\right]$$

Interfacial tensions appear explicitly

Fluid phases configuration and flows of cells within ECM microchannels (a).

Pressure difference - saturation relationships (b, c)

Final system of eqs

$$p^{th} p^{hl} p^{l} \omega^{\overline{dl}} \mathbf{u}_{s}$$

$$p^{th} p^{hl} p^{l} \omega^{\overline{dl}} \mathbf{u}_{s}$$

$$p^{th} p^{hl} p^{l} \omega^{\overline{dl}} \mathbf{u}_{s}$$
Mass balance eqn OXYGEN

$$\begin{bmatrix} s^{t} \frac{\partial \omega^{\overline{d}}}{\partial t} - \nabla \cdot \left(s^{t} b^{\overline{d}} \frac{\partial \nabla}{\partial t} \omega^{\overline{d}}\right) = \frac{1}{\rho'} \left(\omega^{\overline{d}} \frac{d^{t} w}{\partial t} - \frac{d^{t} v}{\partial t}\right) - s^{t} \sqrt{\nabla} \omega^{\overline{d}}$$
Mass balance eqn OXYGEN

$$\begin{bmatrix} \frac{s^{t}}{k_{T}} + \frac{s^{t} (1-s)}{k_{S}} \left[s^{t} + p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right] + s^{t} \frac{\partial s^{t}}{\partial p^{s}} \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{T}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{T}} + \frac{s^{t} (1-s)}{k_{S}} \left[1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{T}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial s^{t}} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) - s^{t} \frac{\partial s^{t}}{\partial s^{t}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) \frac{\partial p^{t}}{\partial s^{t}} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) - s^{t} \frac{\partial s^{t}}{\partial s^{t}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) \frac{\partial p^{t}}{\partial s^{t}} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{tt} \frac{\partial s^{t}}{\partial p^{s}} \right) - s^{t} \frac{\partial s^{t}}{\partial s^{t}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \frac{\partial p^{t}}{\partial s^{t}} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s)}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s^{t}}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^{t}}{\partial p^{s}} \right) \right] \frac{\partial p^{t}}{\partial t} + \left[\frac{s^{t}}{k_{S}} + \frac{s^{t} (1-s^{t}}{k_{S}} \left(1 - s^{t} - p^{t} \frac{\partial s^$$

Linear momentum balance eqn ECM (rate form)

Drimory variables

Numerical solution

Computational procedure





CASE 1: MTS IN VITRO

The evolution of a multicellular tumor spheroid (MTS) in a quiescent, cell culture medium is modelled.



Boundary 1Type: Imposed values $\omega^{\overline{nl}} = \omega_{env}^{\overline{nl}} = 7.0 \cdot 10^{-6}$ $\varepsilon^s = 1 - \varepsilon = 0.05$ $\varepsilon^h = \varepsilon S^h = 0.00$ $\varepsilon^t = \varepsilon S^t = 0.00$ $p^l = 0$ mmHg

Boundary 2

Type: Imposed fluxes Due to the symmetry of the problem there are no normal fluxes.

|--|

	$\boldsymbol{\mathcal{E}}^{s}$	$\boldsymbol{\varepsilon}^{t}$	${oldsymbol{\mathcal{E}}}^h$	p^l	$\omega^{\overline{nl}}$
Red zone	0.05	0.01	0.00	0.00	7·10 ⁻⁶
Blu zone	0.05	0.00	0.00	0.00	7·10 ⁻⁶

CASE 1: MTS IN VITRO



Numerical prediction of the volume fraction of the tumor cells (total and living volume fractions) during 360h (a); mass fraction of oxygen (b).

Optical Imaging of Prostate Tumor in Rat Model: the Fluorescent near-infrared probe (PSS-794) targets the necrotic core of the tumor

Bradley D. Smith et al.

CASE 2: MTS IN VIVO



	σ_{hl} [mN/m]	σ_{tl} (mN/m)	σ_{th} (mN/m)	$a_h ({ m N/m^3})$	$a_t ({ m N/m^3})$	μ^h (Pa s)	μ^t (Pa s)
Case A	72.0	108.0	36.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes 10^1$
Case B	72.0	84.0	12.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes 10^1$
Case C	72.0	72.0	0.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes 10^1$
Case D	72.0	72.0	0.0	$1.5 imes 10^6$	$1.0 imes 10^6$	$3.6 imes10^1$	$3.6 imes 10^1$
Case E	72.0	72.0	0.0	0.0	0.0	$7.2 imes 10^1$	$3.6 imes 10^1$

CASE 2: MTS IN VIVO



Radius [µm]

	σ_{hl} [mN/m]	σ_{tl} (mN/m)	σ_{th} (mN/m)	$a_h ({ m N/m^3})$	$a_t ({ m N/m^3})$	μ^h (Pa s)	μ^t (Pa s)
Case A	72.0	108.0	36.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes 10^1$
Case B	72.0	84.0	12.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes10^1$
Case C	72.0	72.0	0.0	0.0	0.0	$3.6 imes 10^1$	$3.6 imes 10^1$
Case D	72.0	72.0	0.0	$1.5 imes 10^6$	$1.0 imes 10^6$	$3.6 imes 10^1$	$3.6 imes 10^1$
Case E	72.0	72.0	0.0	0.0	0.0	$7.2 imes 10^1$	$3.6 imes 10^1$

CASE 3: TUMOR CORDS

Two blood vessels are considered with the tumor present initially only in one vessel. In a first numerical simulation (S1) the distance between the two vessels is 80 μ m, in a second one (S2) the distance is 100 μ m



(a) Initial conditions of the third case. Yellow shows the axes of the two capillary vessel(b) Geometry and boundary conditions.

CASE 3: TUMOR CORDS

Two blood vessels are considered with the tumor present initially only in one vessel. In a first numerical simulation (S1) the distance between the two vessels is 80 µm, in a second one (S2) the distance is 100 µm



Case 3-S1: Tumor growth from 0 to 20 days

CASE 3: TUMOR CORDS

Two blood vessels are considered with the tumor present initially only in one vessel. In a first numerical simulation (S1) the distance between the two vessels is 80 µm, in a second one (S2) the distance is 100 µm



Volume fractions of the living tumor cells (first column) of the healthy cells (second column) and mass fraction of oxygen (third column) for the case S1.

CASE 4: GROWTH OF MELANOMA

Recently the assumption of a rigid scaffold has been relaxed and the impact of **ECM deformability** can be now properly **taken into account**



Z - axis of cylindrical symmetry

CASE 4: GROWTH OF MELANOMA



CASE 4: GROWTH OF MELANOMA









THCM model young concrete

Conclusions

- The model, even if sophisticated, is reasonably exploitable for real life cases.
- Going from the material scale to the structural one an agreement between the numerical and experimental results is achieved qualitatively and quantitatively.

Perspectives

- The creep rheological model must be enhanced to take into account concrete age (long-term creep).
- Numerical results of the hydration dependent damage model must be confirmed by experiments, which are currently under design.

Tumor growth model

Conclusions

- A multiphase model for tumor growth in the avascular stage has been developed.
- Diffuse interfaces are considered with pressure differences between the three fluids;
- The computational procedure has a modular structure which allows to add new building blocks if needed (c_i, vasculature, T, pH...);

Perspectives

- Modeling of angiogenesis and introduction of vasculature, drugs delivery.
- Extensive validation with experiments.

Thank you for your attention!